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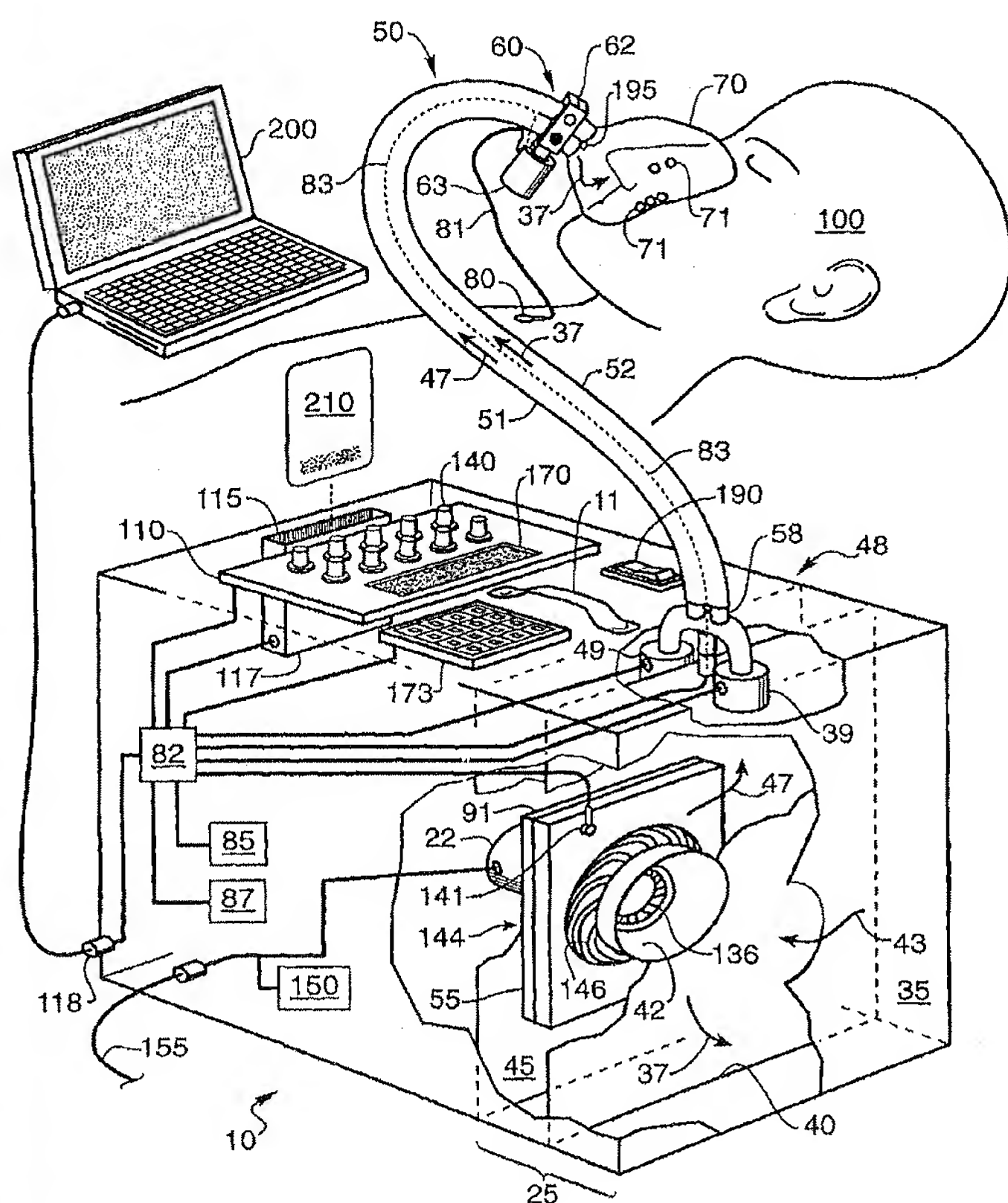
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(54) Title: DUAL-PRESSURE BLOWER FOR POSITIVE AIR PRESSURE DEVICE



(57) Abstract: A gas compression and delivery device for treatment of sleep disorders. The device has a motor, at least one impeller, and two air pressure chambers, each receiving air at a different pressure, one pressure applied to a patient during inspiration and one for expiration. A mask having a dual pressure gas delivery hose and a selector for letting in either the high or low pressure gas depending on the breathing cycle of the patient. The gas pressures are adjustable by means of valves on the separate chambers in the device. At least one sensor on the patient sending data to a controller in the device as to the patient's physiological data which is used to determine the patients breathing treatment needs. The controller may be a microprocessor with memory capability to store patient data for diagnosis and treatment of the patient. Telecommunications by telemetry, or telephony to a remote site allows home use of the device rather than institutional use with health car providers on site. A data card may be used to input and or store data in the device. The controller is capable of instructing the device to treat the patient with a number of different protocols and record the patient's physiological data for diagnosis and treatment purposes.

1

## 2 Dual-Pressure Blower for Positive Air Pressure Device

3

## 4 Background of the Invention

## 5 Field of the Invention

6 This invention relates to a dual pressure pump having at least one impeller  
7 producing two separate pressures in two separate chambers. The dual pressures are used  
8 for positive air pressure treatments in patients with sleep disorders. One pressure is used  
9 during inspiration and one pressure is used during expiration.

10

## 11 Description of the Related Art

12 There are many Bi-Positive Air Pressure (Bi PAP) devices used for treatment of  
13 sleep apnea, and other sleep disorders. These devices mostly use a variable speed motor  
14 with one blower to increase and decrease the air pressure applied to the patient or use  
15 valves to regulate the air pressure applied to the patient.

16 The devices with variable speed motors take a while to change the pressure  
17 applied to the patient, as the motor speed does not change instantaneously between the  
18 inspiration and expiration pressure settings. Similarly valves regulating the pressure in a  
19 chamber have a lag time while pressure is building up or reducing before it reaches the  
20 proper pressure to be applied to the patient.

21 U.S. Patent Number 5,485,850 to Dietz issued January 23, 1996 shows a Bi PAP  
22 device with two separate air supply sources at two different pressures.

23 A device is needed having one unit for supplying dual pressures to the patient  
24 such that there is always a ready supply of air at two different pressures to treat a patient.

25

## Summary of the Invention

The invention comprises a motor with at least one impeller. The impeller or impellers produce a different air pressure in different chambers. A hose transports the air from the chambers to the mask worn by the patient to deliver air at one pressure for use during inspiration and at another pressure during expiration. A valve selects which pressure to allow into the mask depending on if the patient is inhaling or exhaling. There is a means for detecting if the patient is inhaling or exhaling which regulates the valve. There are also means for measuring the airflow into and out of the patient.

A humidifier can adjust the humidity of the air being delivered to the patient.

Altitude adjustments are made to increase or decrease the impeller speed to deliver the correct air pressure to the patient.

The two chambers can have two pressures at adjustable ratios to adjust the inspiration and expiration pressures.

The patient can be monitored by a number of sensors for determining when the patient is inhaling or exhaling. The monitoring sensors can also measure a number of other parameters such as breathing rates, blood oxygen levels, stages of sleep, mask leaks, mask on or mask off, body position and movement of the patient, EEG, EKG, sounds such as snoring, and other information useful for sleep disorder diagnosis and treatment. The information obtained can be used in conjunction with adjusting pressures and times of delivery of air to the patient in real time, adjusting for mask leaks, storing information about the patient for diagnosis and long-term studies, or for alerting health care workers about the patient's condition requiring immediate action.

The sensors can trigger a mask off alarm or detect when the mask is put on to start the power for the motor to supply air to the patient.

1           A controller or microprocessor programmed to evaluate the data from the sensors  
2   on the patient, can make changes to the air pressure applied to the patient, and the timing  
3   thereof. The microprocessor can also store information for later reporting, transmit the  
4   data to recording equipment, or alert health care workers of the patient's condition.

5           Displays can provide data for the number of hours the motor has been on or other  
6   data of interest to the operator.

7 Data cards for input or output of data may be used. Data from the data card may  
8 be sent to a remote site by telemetry, telephony or by mailing the data card.

9           The device may be equipped with anti-rebreathing sensors and apparatus to ensure  
10   fresh air inspiration.

11           The device is portable, light weight and easy to use by a patient without the  
12   assistance of a health care provider such that the device can be used at home and  
13   monitored at a remote location.

## 14

## 15 Objects of the Invention

16           It is an object of the invention to provide a dual air pressure pump with one motor  
17   having at least one impeller.

18           It is an object of the invention to provide accurate pressure control for inspiration  
19   and expiration gas delivery pressures.

20 It is an object of the invention to provide fast transitions between inspiration and  
21 expiration pressures delivered to the patient.

22 It is an object of the invention to provide a portable BiPAP device.

23           It is an object of the invention to provide a multiple purpose device for BiPAP,  
24   CPAP, VPAP, SPAP, PPAP and AutoPAP applications.

25 It is an object of the invention to add humidity to the pressurized air.

1 It is an object of the invention to monitor the patient.

2 It is an object of the invention to measure airflow to and from the patient.

3 It is an object of the invention to record patient data for diagnosis and treatment.

4 It is an object of the invention to provide data storing cards for use in the device.

5 It is an object of the invention to communicate patient condition to remote

6 monitoring equipment and personnel.

7 It is an object of the invention to treat a variety of sleep disorders with a variety of

8 treatments with one device.

9 It is an object of the invention to provide options for several different treatment

10 protocols on one device.

11 It is an object of the invention to provide adjustable settings for individual patient

12 needs and comfort while using the device.

13 It is an object of the invention to provide long term monitoring data of one or

14 more patients for medical studies.

15 It is an object of the invention to display data about the patient or device for ease

16 of reference.

17 It is an object of the invention to provide variable ratios of air pressure for

18 inspiration and expiration.

19 Other objects, advantages and novel features of the present invention will become

20 apparent from the following detailed description of the invention when considered in

21 conjunction with the accompanying drawings.

22

23 Brief Description of the Drawings

24 Fig. 1 is a schematic showing the device with two separate air intakes and two separated

25 impellers.



1 Fig. 2 is a schematic of a second embodiment showing the device with one air intake and  
2 two coaxial impellers.

3 Fig. 3 is a top view of the control panel.

4 Fig. 4 is a side view of a coaxial dual impeller blower in a housing as used in the  
5 schematic of Fig 2.

6 Fig. 5 is a cross sectional side view of one impeller in a housing with a bleed off slot.

7 Fig. 6 is a cross sectional side view of a movable position impeller in a housing.  
8

### 9 Description of the Preferred Embodiments

10 In treating patients having sleep disorders it is frequently required to administer a  
11 Bi-Positive Air Pressure (Bi PAP). In this treatment a first air pressure on the order of 20  
12 cm H<sub>2</sub>O is applied to the patient during inspiration and a second pressure on the order of  
13 3 cm H<sub>2</sub>O is applied to the patient during expiration. Preferably these pressures are  
14 adjustable for the needs of each individual patient. Referring to Fig. 1 a schematic of the  
15 system is shown wherein a gas delivery device 10 supplies gas at two different positive  
16 air pressures to a patient 100. The gas delivery device 10, preferably is small enough and  
17 light weight enough to be portable. The gas delivery device 10 has a carrying handle 11 to  
18 aid in transporting the device.

19 A portable gas delivery device may have a battery 150 for an internal power  
20 supply, a power cord 155 for an outside source of power, or both. The battery 150 may be  
21 rechargeable from the outside power source.

22 A motor 20 receiving power from the battery 150 or an outside power source  
23 through the power cord 155 turns shaft 22. The motor 20 is preferably a brushless DC  
24 motor. Motor with brushes and a commutators produce ozone or NO<sub>x</sub> and other related  
25 particles which would be detrimental if added to the air of the breathing apparatus. The

1 shaft 22 enters the pump housing 25 having a high pressure chamber 45 and a low  
2 pressure chamber 35 which are adjacent, having a barrier 40 therebetween. The shaft 22  
3 turns high pressure impeller blades 46 in the high pressure chamber 45 and turns low  
4 pressure impeller blades 36 in the low pressure chamber 35. The air intake aperture 142  
5 for the high pressure chamber 45 has air filter 90 for filtering intake air stream 43 entering  
6 the high pressure chamber 45. Similarly air intake aperture 132 for the low pressure  
7 chamber 35 has air filter 92 for filtering intake air stream 33.

8 Alternatively the air intake can be a common air intake if the impellers 36 and 46  
9 in Fig. 1 are turned around such that the air intake is between them and the air output  
10 would be to chambers which are separate.

11 The ratio of the high pressure in chamber 45 to the low pressure in chamber 35 is  
12 fixed by the relative size or position of the impeller blades. The ratio can be changed by  
13 varying a number of parameters including the relative size of the impellers, the gaps  
14 between the impellers and the housings, the size of the openings in the housings for  
15 admitting air from the impellers, or by other variables. The ratios may be adjustable or  
16 fixed. Generally for one patient the ratio of the inspiration pressure to the expiration  
17 pressure can remain fixed. It may be necessary to adjust the ratios for different patients or  
18 adjust the ratios for the same patient over time.

19 A humidifier 55 may be used to adjust the humidity of the air being supplied to  
20 the patient. The humidifier 55, as shown in the dual pressure gas delivery device 10, is in  
21 front of the high pressure air intake aperture 142 to supply moisturized air for inspiration.  
22 The humidifier 55 may be placed in other locations for supplying high pressure and/or  
23 low pressure moisturized air to the patient. A humidity control 140 to select the desired  
24 humidity is located on the control panel 110 and works in conjunction with humidity

1 sensors 141 in housing 25 and the controller or microprocessor 82 to keep the humidity at  
2 a desired setting.

3 In a second embodiment shown in Figs. 2 and 4 the motor 20 has a shaft 22 with  
4 impellers 136 of a first radius and impellers 146 of a second radius coaxially mounted on  
5 the shaft 22. There is one air intake 144 to the impellers 136, 146 for producing two  
6 streams of air, one at a high pressure, air stream 47 in chamber 45 and one at a low  
7 pressure, air stream 37 in chamber 35. Since this embodiment has only one air intake 144  
8 only one air filter 91 and one humidifier 55 are required. Fig. 4 shows a more detailed  
9 view of the motor 20, high pressure impeller 146 and low pressure impeller 136 on shaft  
10 22 in relation to housing 25. The intake air 43 enters housing 25. The low pressure  
11 impeller 136 discharges low pressure air 37 into low pressure chamber 35 and the high  
12 pressure impeller 146 discharges high pressure air 47 into the high pressure chamber 45.

13 In a third embodiment, as shown in Fig. 5, the motor 20 has shaft 22 attached to  
14 impeller 146. The housing has an annular slot 30 in the housing adjacent to impeller 146  
15 to let air of a lower pressure into chamber 35. Intake air 43 is acted on by impeller 146  
16 creating a high pressure air 47 in chamber 45 and low pressure air 37 in chamber 35. The  
17 annular slot 30 may be continuous or divided into sections.

18 The motor 20 in the three embodiments turns one or more impellers on shaft 22  
19 for steadily supplying a high pressure air in the high pressure chamber 45 and a low  
20 pressure air chamber 35. On one embodiment the motor speed is fixed to supply a  
21 constant pressure in the high and low pressure chambers 45 and 35. In another  
22 embodiment a variable speed motor can be used to such that as the motor 20 speeds up or  
23 slows down a higher or lower volume of air is pumped and both the high pressure and  
24 low pressure are simultaneously adjusted upward or downward. A change in the motor  
25 speed can be used to make a pressure adjustment to the high pressure chamber 45 or low



1 pressure chamber 35 when the ratio of the pressures is fixed but a variation or adjustment  
2 of the pressures in the chambers is called for. In this manner the high pressure and/or low  
3 pressure can be varied with changes in motor speed. Devices having one impeller and one  
4 pressure chamber would have to make large changes in motor speed and have a lag time  
5 to change speed and thereafter the pressure in the pressure chamber. A dual pressure  
6 impeller or two impellers with two pressure chambers do not require any motor speed  
7 change to change the pressure from high to low. However, adjustments to the pressure  
8 can still be effected by changing the motor speed.

9 In a fourth embodiment shown in Fig. 6 an actuator 300 moves actuation rod 310  
10 up or down by a small distance as shown by arrows 315. Actuator rod 310 is attached to  
11 slider 320 which moves up or down in housing 325. Slider 320 carries motor 20 and  
12 impeller 346 up and down adjusting the clearance distance 350 between the impeller and  
13 housing 325. With a larger clearance distance 350 the leakage rate of compressed air goes  
14 up reducing the air pressure in chamber 345. With a smaller clearance distance 350 the air  
15 pressure in chamber 345 goes up. The air intake 43 supplies air for the impeller 346 to  
16 pump up to the desired pressure in chamber 345. The actuator 300 can quickly and  
17 accurately adjust the clearance 350 between the impeller 346 and housing 325 thus  
18 quickly adjusting the pressure chamber 345 without changing the motor 20 speed.

19 The actuator 300 may be hydraulically, mechanically, electrically,  
20 electromechanically, or piezoelectrically driven. Any means for quickly and accurately  
21 moving the actuator rod 310 will allow the invention to be practiced.

22 The embodiment in Fig. 6 shows motor 20 on slider 320 however other  
23 embodiments where the motor is fixed and the actuator 300 only moves the impeller 346  
24 are within the scope of the invention.

1 In all of the embodiments shown the motor 20 has shaft 22 connected to impeller  
2 an impeller, however in other embodiments the impellers can be on the outside of a  
3 rotating motor housing eliminating the need for a shaft 22.

4 Altitude compensation is required for the impeller speed to increase or decrease to  
5 bring the pressure up to the desired level. A pressure altitude sensor 85 senses the altitude  
6 and reports it to the controller 82; the controller then adjusts the motor speed accordingly.  
7 Altitude compensation can be controlled by a pressure transducer.

8 In the embodiments shown in Figs. 1 and 2 if the pressure in the high pressure  
9 chamber 45 is kept at a pressure higher than needed for the patient 100 and the pressure in  
10 the low pressure chamber 35 is kept at a pressure higher than needed for the patient then a  
11 high pressure adjustment valve 49 and a low pressure adjustment valve 39 may be used to  
12 adjust the pressure of the air being delivered to the patient. The high pressure air flow 47  
13 from the high pressure chamber 45 and the low pressure air flow 37 from the low pressure  
14 chamber 35 may thereby be regulated. The high and low pressure valves 49 and 39  
15 respectively may be controlled by a controller or microprocessor 82 or set manually on  
16 control panel 110 as inspiration pressure control 120 and expiration pressure control 125.

17 Alternatively in another embodiment the motor 20 speed is adjusted to provide the  
18 desired pressure in the high pressure chamber 45 and in the low pressure chamber 35  
19 eliminating the need for valves.

20 The outlet nozzle 48 is a split nozzle extending from the housing 25 over the  
21 housing barrier 40 such that both high pressure air 47 the adjacent low pressure air 37  
22 flow in their respective halves of the nozzle to a split coupler 58 having two sides.

23 A dual pressure hose 50 connects to the coupler 58. The dual pressure hose 50 has  
24 a high pressure side 51 and a low pressure side 52 for transporting the high pressure gas  
25 47 and low pressure gas 37 to the mask 70.

1           Alternatively the dual pressure 50 hose can be a small diameter hose inside of a  
2   larger diameter hose for transporting the separate pressures from the housing to the mask,  
3   or two separate hoses can be used.

4           A valve 60 at the entrance to the mask 70 alternately selects the high pressure air  
5   47 or low pressure air 37 to be supplied to the patient 100 depending on if the patient is  
6   inhaling or exhaling. When the patient 100 is inhaling the valve 60 selector 62 blocks the  
7   low pressure air in the low pressure portion 52 of hose 50 and admits the high pressure  
8   from the high pressure portion 51 of hose 50. Similarly when the patient 100 is exhaling  
9   the valve 60 selector 62 blocks the high pressure portion 51 of hose 50 and admits low  
10   pressure air. An actuator 63 moves the selector 62 based on information about the  
11   patient's breathing obtained from sensors 71 in the mask 70 and or sensors 80 placed on  
12   the patient 100. The controller or microprocessor 82 determines when the patient 100 is  
13   inhaling or exhaling from the data provided and positions the actuator 63 accordingly by  
14   sending it signals over lead 83.

15           The valve 60 may be a split butterfly valve, a gate valve or any other type of valve  
16   for selectively admitting only one pressure.

17           In one embodiment for controlling the pressure to the mask 70 a valve 60 such as  
18   a butterfly valve can be partially open to the high pressure chamber 45 and partially open  
19   to the low pressure chamber 35 simultaneously, resulting in a mix of between 0 and 100%  
20   of each pressure to select an intermediate pressure to the mask. The valve 60 can be  
21   quickly activated to any setting to provide any pressure between the high pressure in the  
22   high pressure chamber 45 and the low pressure in the low pressure chamber 35.

23           Alternatively a hose 50 with one lumen can be used and the valve 60 for selecting  
24   high or low pressures can be at the outlet nozzle 48. The hose 50 will then contain either a  
25   high pressure air flow 47 or a low pressure air flow 37 to the mask 70.

1           The sensors 71 used for supplying information about the patient's breathing to the  
2   controller or microprocessor 82 may be imbedded in the perimeter of the mask 70 or on  
3   the mask surface. Such a mask 70 and the types of sensors used are described in the  
4   applicant's copending patent application titles Bio-Mask serial number 09/465,054 filed  
5   December 16, 1999 which is hereby made a part hereof and incorporated herein by  
6   reference.

7           In one embodiment a sensor 71 on the mask or in the dual pressure gas delivery  
8   device 10 can detect when breathing into the mask begins or when mask 70 is donned by  
9   a patient to automatically turn on the power to the motor 20.

10          The sensors 71 can detect leaks or drops in pressure and send signals to  
11   microprocessor 82 to increase the pressure sent to the mask 70 to compensate for the  
12   leaks.

13          Sensors 71 can also detect the expiration gases to see if the patient is rebreathing  
14   his breath. The microprocessor 82 is programmed to adjust valves in the mask or  
15   pressures to the mask to prevent rebreathing.

16          Other sensors on the patient such as sensor 80 on the patient's chest may be used  
17   for supplying information about the patient's breathing to the controller or  
18   microprocessor 82.

19          Some means for the detection of inspiration and expiration are shown in  
20   applicant's PCT applications WO 98/50095, entitled Controlling Gas of Drug Delivery to  
21   a Patient, international filing date May 7 1997, and in WO 97/16216 entitled Apparatus  
22   for Gas Delivery, international filing date October 31, 1996. Other patents teaching  
23   breathing measurements are U.S. patents 4,440,177 and 4,463,764. All of the above  
24   patents and applications are attached hereto and incorporated herein by reference.

1           Other means for detecting breathing are by measuring air flow movements to the  
2   mask 70 from the air supply such as sensors like 195 placed at the entrance to the mask  
3   70. The sensors 195 may be laser sensors, radar Doppler sensors, ultrasonic sensors,  
4   ultrasound techniques, pitot tubes, or other electronic or mechanical means for measuring  
5   the air passing the sensor. Other means for measuring air flow rates and breathing are  
6   available such as shown in U.S. patents 5,038,733 entitled Flow Meter System issued  
7   Aug 13, 1991 and 4,796,639 entitled Pulmonary Diagnostic System, issued Jan 10, 1989  
8   both of which are attached hereto and made a part hereof by reference.

9           The dual pressure gas delivery device 10 can be used to select only high pressure  
10   gas at all times to provide treatment of Continuous Positive Air Pressure (CPAP) with  
11   CPAP protocols. Similarly, with suitable programming of the controller 82, the dual  
12   pressure gas delivery device 10 can be used for Variable Positive Air Pressure (VPAP)  
13   treatment protocols, Sleep linked Positive Air Pressure (SPAP) treatment protocols,  
14   Proportional Positive Air Pressure (PPAP) treatment protocols, Auto Positive Air  
15   Pressure (AutoPAP) or other treatment protocols by using the protocol selection feature  
16   175 on the control panel 110 and having the controller 82 programmed for delivering gas  
17   at the proper gas pressures at the proper times.

18           In some treatment protocols there is a ramp time where the pressure is slowly  
19   increased to the desired pressure for treatment over time as the patient falls asleep. The  
20   dual pressure gas delivery device 10 has a controller/ microprocessor 82 which can be  
21   programmed for ramp times and pressures as required by the patient. A ramp time control  
22   knob 130 on the control panel can also be used to select the ramp times. Ramp delay  
23   times are used in conjunction with ramp times. The ramp delay times allow a time before  
24   the ramp up of pressure begins, allowing the patient to fall asleep before the treatment



1 begins. The ramp delay times can be selected on the control panel 110 by ramp delay time  
2 control selector 135.

3 The ramp times, ramp delay times and other parameters can be programmed into  
4 the controller/microprocessor 82 by means of information stored on a data card 210  
5 inserted into a data card port 115. Alternatively the controller/microprocessor 82 may be  
6 programmed by a computer 200 and the information transferred to the  
7 controller/microprocessor 82 through computer input output plug 118. The computer 200  
8 may be remotely located at a hospital or sleep clinic and connected through the internet  
9 by wire or wireless phone systems or positioned adjacent the dual pressure gas delivery  
10 device 10.

11 Alternatively a keypad 173 can be used to enter data into the  
12 microprocessor/controller 82 for patient data information, or to select times, pressures or  
13 other parameters for running the dual pressure gas delivery device. A menu on display  
14 170 driven by controller 82 may prompt the user to enter data for settings by use of the  
15 keyboard 173.

16 Other settings on the control panel 110 are for comfort settings 180 in which the  
17 temperature, pressure, humidity and timing of the application of pressurized air to the  
18 patient is controlled. The comfort setting may also be stored on the data card 210 or in the  
19 controller 82, or computer 200 to provide the best comfort setting for the type of  
20 treatment individualized for the patient.

21 The control panel 110 or other portion of the device can have an on off switch 190  
22 easily accessible by the patient for turning the device 10 on and off.

23 The control panel can have a display panel 170 such as an LCD for displaying  
24 information about the patient, the performance parameters of the dual pressure gas  
25 delivery device 10, such as an hour meter for how long the motor 20 has been on, an

1 elapsed time at pressure meter, an elapsed running time meter or other information. Such  
2 information can be selected for display by a selection button on the control panel 110, by  
3 a touch screen LCD or by other means. The information selected can be transmitted from  
4 the controller/microprocessor 82, to the display panel 170 or can be recorded or stored on  
5 a smart card 210 or the microprocessor 82 and can be transmitted to a computer 200.

6 Different sleep disorder treatments use different trigger points to start the  
7 application of the high pressure during inspiration. A spontaneous trigger point measures  
8 the patient's spontaneous respiratory effort to trigger the application of gas to the patient  
9 when he starts to inhale. A timed trigger point uses a predetermined rate to trigger the  
10 application of gas to the patient.

11 Adjustable trigger points can be set in the controller 82 or on the control panel 170  
12 to vary the pressures at which the patient begins to receive air either during inspiration or  
13 expiration

14 Poor synchronization between the patient's and the machine's 'breathes' lead to  
15 an unwanted increase in the work of breathing by the patient, reduced comfort and,  
16 subsequently detrimental/reduced therapy. Therefore it is important to have sensors 71,  
17 80 providing data to a controller 82 for application of the proper pressure at the proper  
18 time to treat the patient 100. It is also important in BiPAP applications for the air supply  
19 to be at the right pressures in the mask 70 at the right time. In order to accomplish this  
20 one motor 20 spinning at one rate can supply two pressures to a mask 70 with a selector  
21 62 alternating between the high and low pressures as the patient inhales and exhales. The  
22 motor speed can be increased or decreased to provide higher or lower pressures for  
23 inhaling and exhaling.

24 Communications from the sensors 71, 80 can be by leads 83, 81 respectively or by  
25 telemetry to the controller 82.

1           The controller 82 can be programmed remotely by telemetry, through transmitter  
2 receiver 87, or by wire to a port 118 to plug in a data line from a computer 200 to the  
3 controller 82. The controller 82 can also be programmed by a data card 210 inserted into  
4 data card port 115 to transfer instructions to the controller 82.

5           The port 118 can also be used to receive data from the controller 82 obtained from  
6 the sensors 71, 80 and send it to the computer 200 for use by health care workers.

7           For example the sensors 71, 80 may collect data about breathing volumes,  
8 breathing rates, breathing times, blood oxygen, EEG, EKG, EOG, EMG, patient pulse,  
9 patient temperature, snoring, position of the patient, sleep stages, patient movement, mask  
10 pressures, mask leakage, and other relevant data such as would be collected for a  
11 Polysomnogram (PSG). Such data for treating the patient may be sent by leads or by  
12 telemetry to the controller 82 for processing and storage. Patient data may be used to treat  
13 the patient in real time or be stored and studied at a later time. The data may be  
14 transmitted to a computer 200 at a remote location such as a doctor's office or hospital for  
15 remotely monitoring the patient. The computer 200 can store data about the patient which  
16 can be presented to a health care provider to diagnose or treat the patient. The data stored  
17 about a patient can be used over long term studies and can print out progress reports about  
18 the patient. Further if a patient is taking part in a study with a group of other patients the  
19 data is readily available to be used in the data for the study.

20           Connections to the computer 200 can be by telemetry such as by Blue Tooth®, a  
21 cell phone data transmittal protocol, or over telephony networks through data port 118.

22           Telemetry devices used to transmit and store multiple channels of data are  
23 available under the trade name Siesta® by Compumedics Inc. Abbotsford, VIC,  
24 Australia.

1           The dual pressure gas delivery device 10 is preferably compatible with Telemed®  
2   or other remote medical systems such that the patient can use the dual pressure gas  
3   delivery device 10 at home and still have the support of health care providers located  
4   remotely. This device will help free sleep disorder patients from having to be at a hospital  
5   or other health care facility while being treated or tested.

6           Other means for data storage are by a data card or smart card 210 which can store  
7   data about a patient, or provide data about the patient or for programming the controller  
8   82. The data card or smart card is inserted into card port 115 to access the dual pressure  
9   gas delivery device 10.

10          Input means for data or selections to control the dual pressure gas delivery device  
11   10 through control panel 110 can be by selecting settings from any array of control knobs  
12   on the control panel 110, by a menu driven touch screen on display 170 in conjunction  
13   with controller 82, or by other input/output devices as are currently known and used in the  
14   art.

15          A sensor or sensors in or on a mattress the patient is on may be connected to the  
16   controller 82 to provide data about patient movements and activity rates.

17          There is a need for a mask off alarm or mask leak alarm to tell the patent or health  
18   care worker that the mask is not delivering air to the patient properly. Such detectors are  
19   taught in the patents incorporated herein by reference. When the mask off or mask leak  
20   alarm 165 is activated the mask should be checked and the alarm deactivated. Sensors 71  
21   in the mask 70 can detect if the mask has come off of the patient and send a signal to the  
22   microprocessor 82. The microprocessor can sound an alarm 165 or alert a health care  
23   worker that the mask is off. The microprocessor 82 may shut down the motor 20 if mask  
24   70 is off.

1           The dual pressure gas delivery device 10 can be used for monitoring and treatment  
2   of many sleep disorders. The computer 200, microprocessor 82 or data card 210 can store  
3   date about the duration, start times and stop times of the treatment, the pressures used, air  
4   flow rates and patient data such as heart rates, blood oxygen rates, snoring, patient  
5   movement and other polysomnogram data useful in diagnosing and treating patients.

6           Obviously, many modifications and variations of the present invention are  
7   possible in light of the above teachings. It is therefore to be understood that, within the  
8   scope of the appended claims, the invention may be practiced otherwise than as  
9   specifically described.

10



1 What is claimed:

2 1. A dual pressure gas delivery device comprising:

3 a motor having a shaft extending from the motor, the shaft having at least one

4 impeller for producing a first air pressure and a second air pressure,

5 a housing having a first chamber and a second chamber wherein the first air

6 pressure enters the first chamber, and the second air pressure enters the second chamber,

7 each chamber having an air exhaust aperture such that air having a first pressure

8 exits the air exhaust aperture of the first chamber and air having a second air pressure

9 exits the air exhaust aperture of the second chamber.

10

11 2. A gas delivery device as in claim 1 wherein:

12 one impeller on the shaft increases the pressure of the air for both chambers,

13 the housing has a slot along the length of the impeller leading to the first chamber

14 for providing a first air pressure in the first chamber,

15 the housing has an opening at the end of the impeller for providing a second air

16 pressure in the second chamber.

17

18 3. A gas delivery device as in claim 1 wherein:

19 a first impeller and a second coaxial impeller produce the first and second air

20 pressures introduced to the first and second chambers at the ends of the impellers.

21

22 4. A gas delivery device as in claim 1 wherein:

23 two impellers on different portions of the shaft produce the first and second air

24 pressures introduced to the first and second chambers at the ends of the impellers.

25

1     5.     A gas delivery device as in claim 1 comprising:  
2             a mask for applying gas to a patient,  
3             a means for transporting the air from the first chamber and the second chamber to  
4     the mask,  
5             a means for selecting either the first air pressure or the second air pressure to be  
6     admitted to the mask.

7  
8     6.     A gas delivery device as in claim 5 wherein:  
9             the means for selecting either the first air pressure or the second air pressure to be  
10    admitted to the mask comprises an actuator, attached to the means for transporting the air  
11    to the mask, for moving a selector to block the air from one of the chambers while  
12    allowing the air from the other chamber to pass.

13  
14    7.     A gas delivery device as in claim 6 wherein:  
15             a means for instructing the actuator to select an air pressure such that a high air  
16    pressure is applied to the mask during inspiration and a low pressure is applied to the  
17    mask during expiration.

18  
19    8.     A gas delivery device as in claim 7 wherein:  
20             the means for instructing the actuator to select an air pressure comprises a  
21    controller sending signals to the actuator, and at least one sensor for obtaining  
22    information from the patient about his breathing such that the controller can process the  
23    information to determine if the patient is inhaling or exhaling and send the signals to the  
24    actuator accordingly.

25

1     9.     A gas delivery device as in claim 1 having:  
2             a mask for applying gas to a patient,  
3             a means for transporting the air from the first chamber and the second chamber to  
4     the mask,  
5             a means for selecting a portion of the first air pressure and a portion the second air  
6     pressure so that they can be mixed to create a third air pressure to be admitted to the  
7     mask.

8  
9     10.    A gas delivery device as in claim 9 wherein:  
10            the means for selecting a portion of the first air pressure and a portion the second  
11    air pressure so that they can be mixed to create a third air pressure to be admitted to the  
12    mask comprises a butterfly valve for simultaneously partially blocking the first air  
13    pressure and partially blocking the second air pressure to derive a third air pressure.

14  
15    11.    A gas delivery device as in claim 1 having:  
16            a means for varying the ratio of pressures in the high pressure chamber and low  
17    pressure chamber.

18  
19    12.    A gas delivery device as in claim 1 having:  
20            a means for varying the speed of the at least one impeller to change the pressure in  
21    the high pressure chamber and in the low pressure chamber.

22  
23    13.    A gas delivery device as in claim 1 wherein:  
24            a humidifier adds humidity to the air in at least one chamber.

25

1 14. A gas delivery device as in claim 1 having:  
2 an air filter filters the air of at least one chamber.  
3

4 15. A gas delivery device as in claim 1 wherein:  
5 a handle on the device for ease of transport.  
6

7 16. A gas delivery device as in claim 1 wherein:  
8 a pressure adjustment valve on the first air chamber exhaust aperture allows for  
9 adjusting the air pressure exiting the chamber.  
10

11 17. A gas delivery device as in claim 16 wherein:  
12 a pressure adjustment valve on the second air chamber exhaust aperture allows for  
13 adjusting the air pressure exiting the chamber.  
14

15 18. A gas delivery device as in claim 17 wherein:  
16 a first actuator controls the pressure adjustment valve for the pressure on the first  
17 chamber,  
18 a second actuator controls the pressure adjustment valve for the pressure on the  
19 second chamber, and  
20 both the first and second actuators are controlled by a controller.  
21

22 19. A gas delivery device as in claim 8 wherein:  
23 a pressure adjustment valve on the first air chamber allows for adjusting the air  
24 pressure exiting the chamber.  
25

1     20.     A gas delivery device as in claim 19 wherein:

2             a pressure adjustment valve on the second air chamber allows for adjusting the air  
3     pressure exiting the chamber.

4  
5     21.     A gas delivery device as in claim 20 wherein:

6             a first actuator controls the pressure adjustment valve for the pressure on the first  
7     chamber,

8             a second actuator controls the pressure adjustment valve for the pressure on the  
9     second chamber, and

10            both the first and second actuators are controlled by the controller.

11

12     22.     A gas delivery device as in claim 5 wherein:

13            the device has a means for selecting the pressure of the high pressure air delivered  
14     to the mask.

15

16     23.     A gas delivery device as in claim 5 wherein:

17            the device has a means for selecting the pressure of the low pressure air delivered  
18     to the mask.

19

20     24.     A gas delivery device as in claim 5 wherein:

21            the device has a means for selecting ramp times and ramp time delays for the air  
22     delivered to the mask.

23



1

2 25. A gas delivery device as in claim 5 wherein:

3 the device has a means for selecting the protocol used for delivering air to the  
4 mask such that different treatments can be applied to the patient with the same device.

5

6 26. A gas delivery device as in claim 5 having:

7 a data card port connected to a controller such that a data card inserted into the  
8 data card port can send data to and receive data from the controller.

9

10 27. A gas delivery device as in claim 5 wherein:

11 an input output data port connected to a controller such that data can be send data  
12 to and receive from the controller at a remote site form the device.

13

14 28. A gas delivery device as in claim 5 wherein:

15 a transmitter and receiver connected to a controller such that data can be sent to  
16 and received from the controller.

17

18 29. A gas delivery device as in claim 5 wherein:

19 a keypad connected to a controller enters data to the controller such that settings  
20 for the controller are selected.

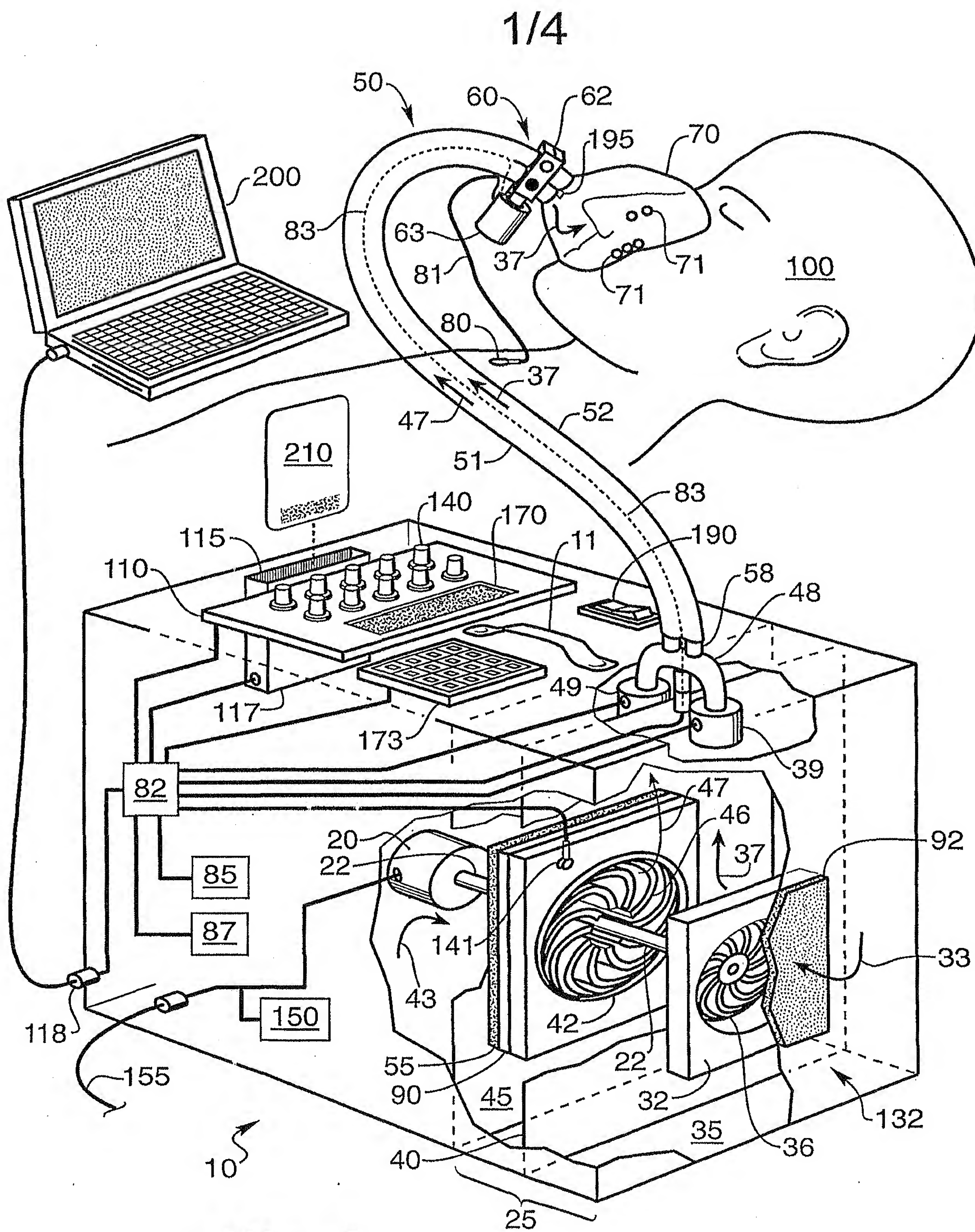
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22 30. A gas delivery device as in claim 5 wherein:

23 a control panel on the device connected to a controller such that data can be sent  
24 to and received from the controller from the control panel.

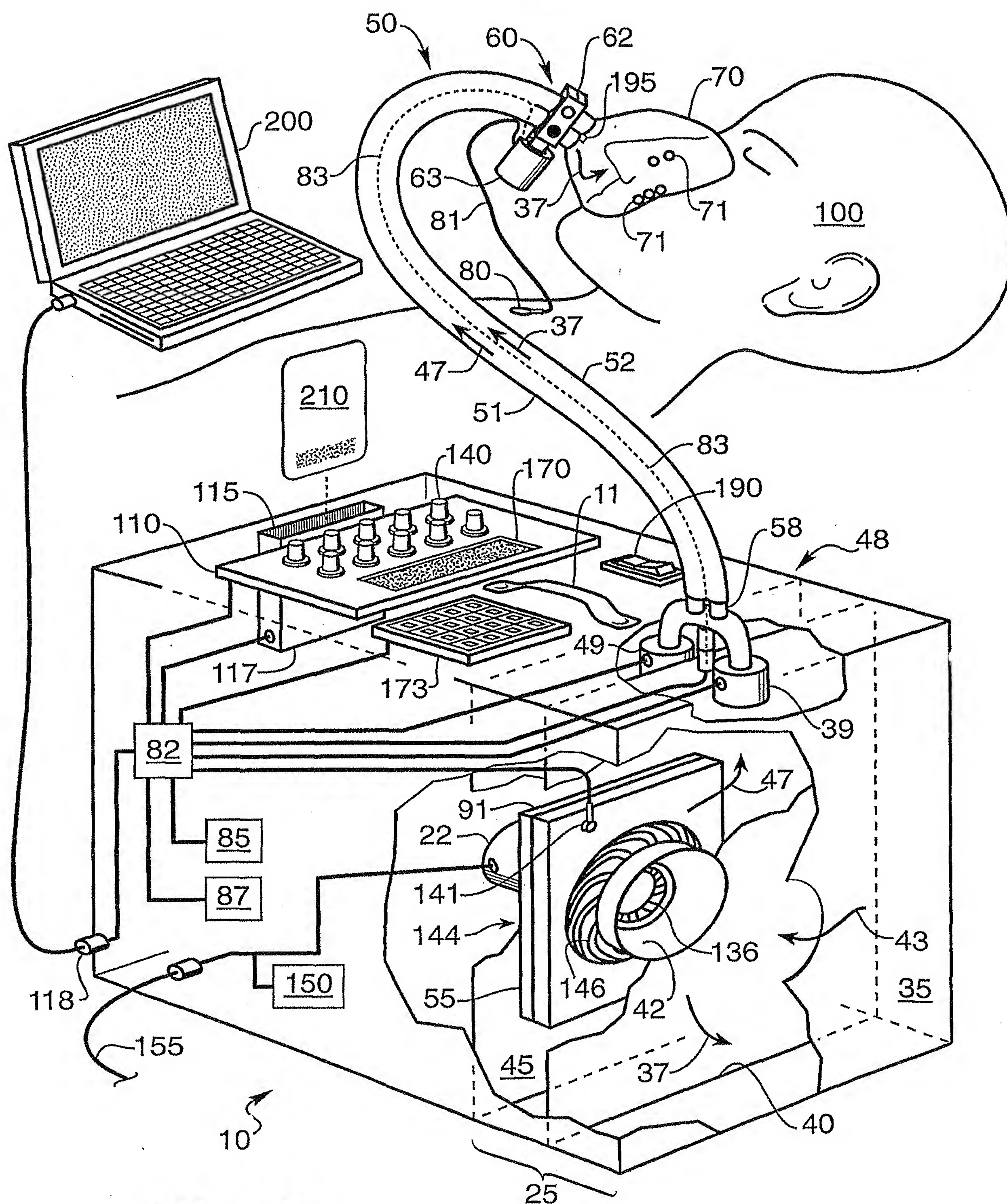
25

- 1     31.     A gas delivery device as in claim 30 wherein:  
2             the control panel has an LCD display. 32.     A gas delivery device as in claim 1  
3     wherein:  
4             the motor is a brushless DC motor such that no ozone or NOx is produced.  
5  
6     33.     A gas delivery device as in claim 1 having:  
7             a means for tracking elapsed time.  
8  
9     34.     A gas delivery device as in claim 33 having:  
10            a means for displaying elapsed time.



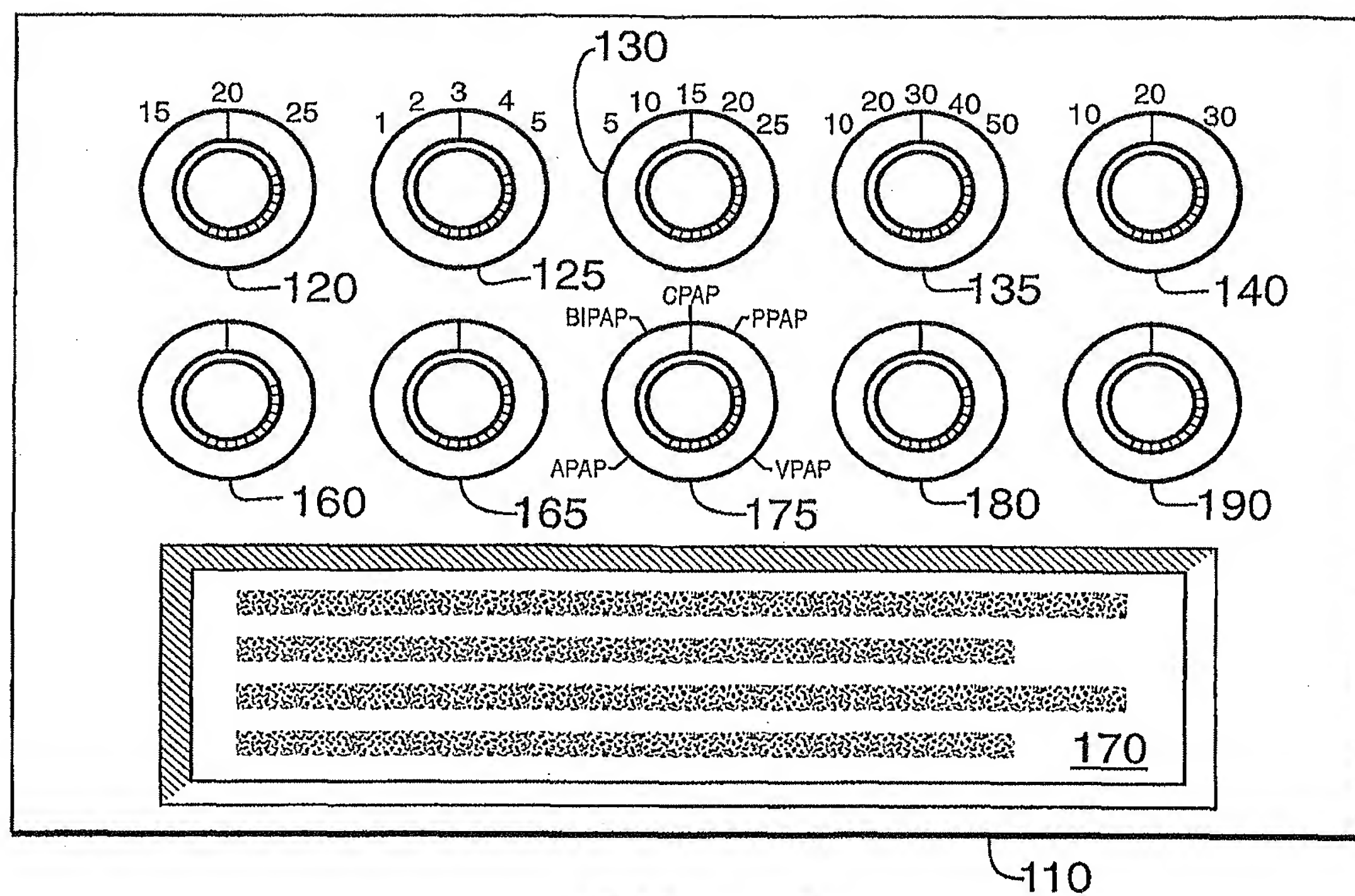
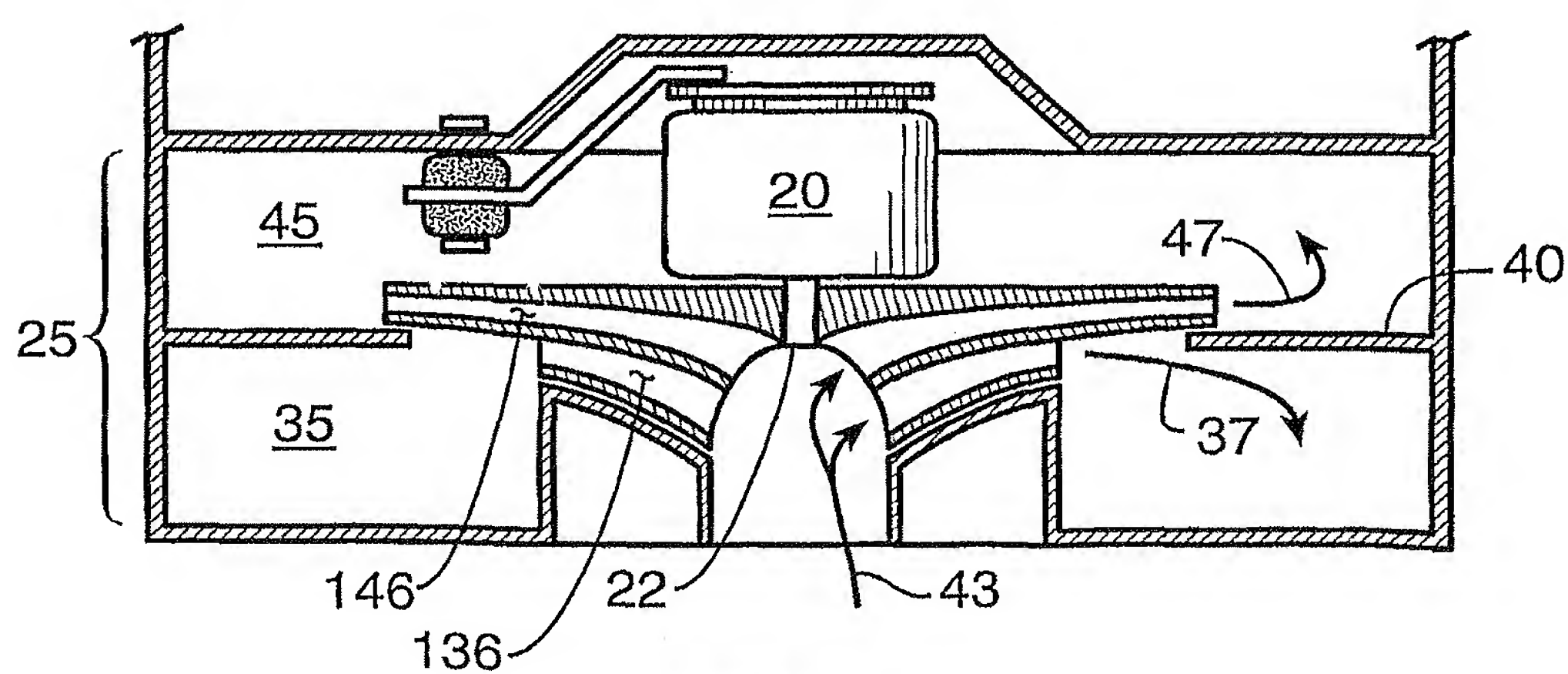
*Fig. 1*

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**Fig. 2**

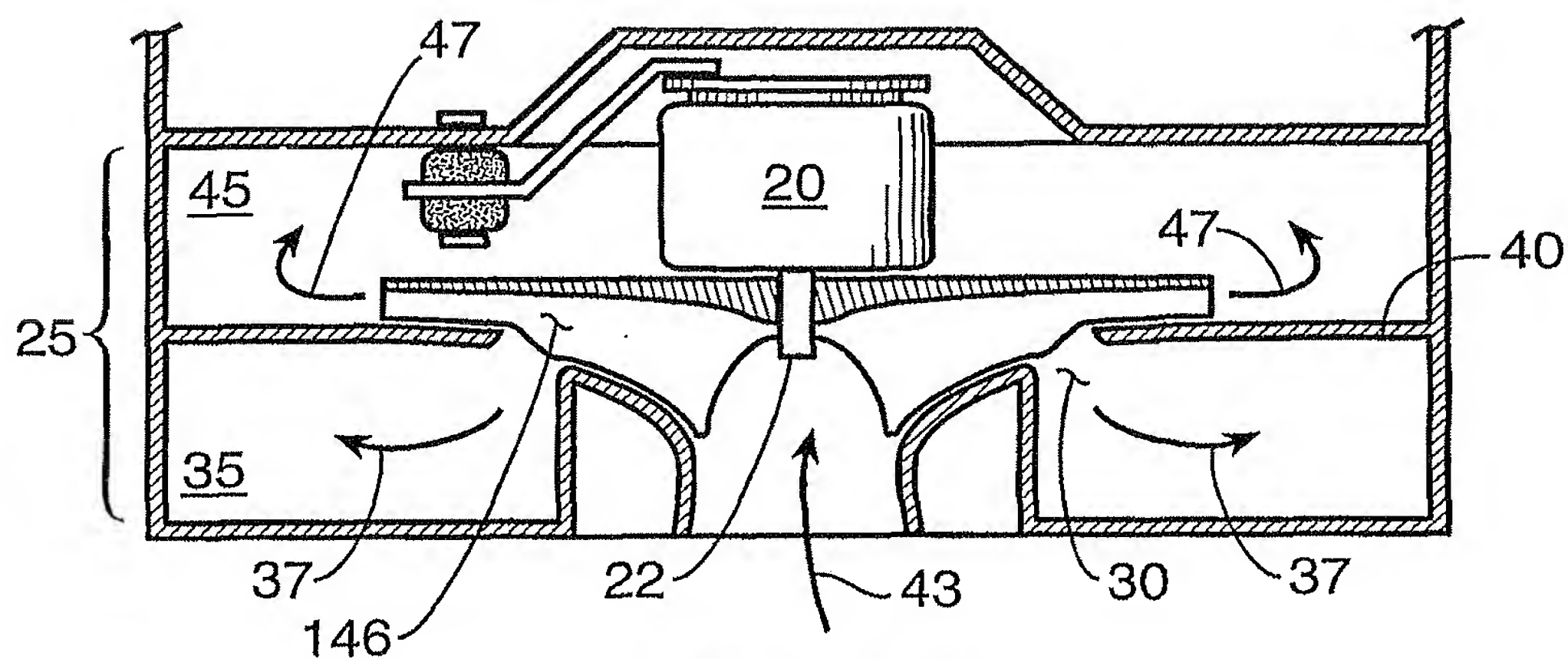
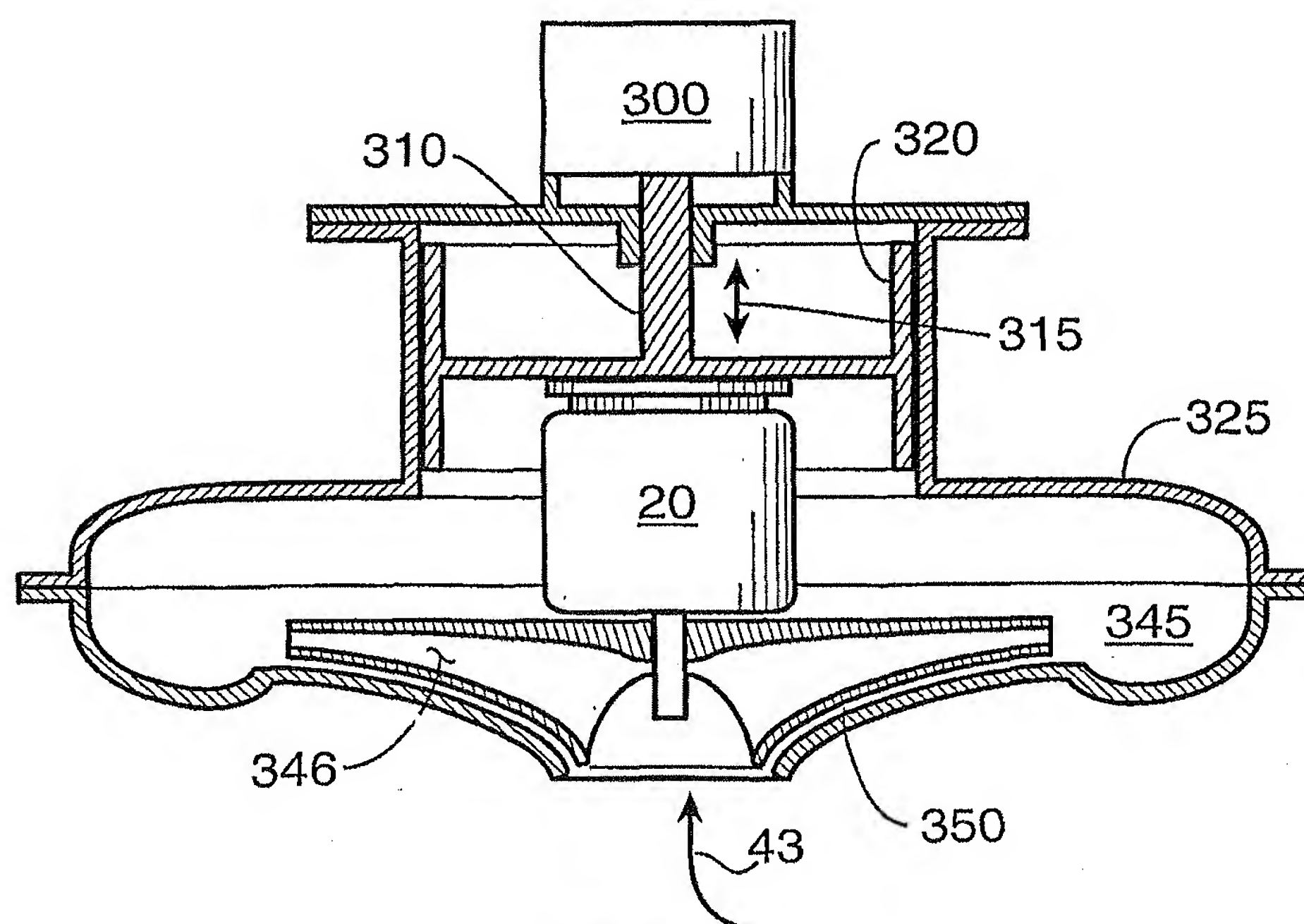


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*Fig. 3**Fig. 4*



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*Fig. 5**Fig. 6*

## INTERNATIONAL SEARCH REPORT

International application No.

PCT/AU01/00196

**A. CLASSIFICATION OF SUBJECT MATTER**

Int. Cl. 7: A61M 16/00

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

DWPI + keywords; dual twin two chamber reservoir impeller impellor pump rotor blower gas air oxygen etc

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 95/32753 A (DRANEZ ANSTALT) 7 December 1995	
A	US 5848538 A (TISCHER) 15 December 1998	

☐ Further documents are listed in the continuation of Box C
 ☒ See patent family annex

* Special categories of cited documents:	
"A" document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E" earlier application or patent but published on or after the international filing date	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O" document referring to an oral disclosure, use, exhibition or other means	"&" document member of the same patent family
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

30 April 2001

Date of mailing of the international search report

3 - MAY 2001

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INTERNATIONAL SEARCH REPORT  
Information on patent family members

International application No.  
PCT/AU01/00196

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report				Patent Family Member			
WO	95/32753	AU	26218/95	EP	762907	US	5988166
		ZA	9504452				
US	5848538	AU	95859/98	EP	1036292	WO	99/24767
END OF ANNEX							